

# Surface Sensitive Techniques

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# Outline

We will look mainly at the following techniques:

- Surface plasmon resonance (optical).
- Quartz crystal microbalance (mechanical).
- Impedance spectroscopy (electrical).



#### **Surface Sensitive Techniques**

Detect <u>anything</u> that binds to a surface! Several instruments exist, most are based on optical measurements, some mechanical and also a few other.

The techniques will be used in the projects!





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#### What is a Plasmon?

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Physical understanding: *Plasmons are collective oscillations in the free electrons of metals.* 

Mathematical understanding: *Plasmons are solutions to Maxwell's equations for certain metal-dielectric geometries.* 

For a metal nanoparticle, the polarization enhanced at certain frequencies of light. For noble metals, this occurs in the visible region, which gives strong colors.

The *Lycurgus Cup* is the oldest example (year ~400) of this kind of staining.

We will dig a bit more into plasmons, but fear not, you do not have to learn the physics in detail!



British Museum http://www.britishmuseum.org/





Ag, Au, Cu (60%, 30%, 10%) in glass

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# **Absorption and Scattering**

The polarizability ( $\alpha$ ) of the particle determines the *absorption* and *scattering* cross sections ( $\sigma$ ). The *extinction* is the sum of absorption and scattering.

For gold nanoparticles (small and spherical): Blue light is absorbed (true for all gold). Green light is absorbed and scattered (by the plasmon). Red light is transmitted (low extinction).

$$\sigma_{\text{ext}} = k \operatorname{Im}(\alpha)$$
$$\sigma_{\text{sca}} = \frac{k^4}{6\pi} |\alpha|^2$$

$$\sigma_{\rm abs} = \sigma_{\rm ext} - \sigma_{\rm sca}$$

Here k is the incident wavevector  $(k = 2\pi/\lambda)$ . The polarizability is a <u>volume</u> and the cross sections are <u>areas</u> (shadows)!



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British Biocell International http://www.bbisolutions.com/

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### **Electrostatic Approximation**

By considering the electric field of light as static, the polarizability can be calculated easily for a sphere:

$$\alpha_{0} = 3V \frac{\varepsilon(\lambda) - \varepsilon_{m}}{\varepsilon(\lambda) + 2\varepsilon_{m}} \int_{Classical Electrodynamics Wiley 1999}^{Jackson}$$

(1)

This is valid for particles that are small compared to the wavelength of light (<50 nm).

Here  $\varepsilon$  is again (relative) permittivity, but now at optical frequencies.

For simple transparent materials,  $\varepsilon$  is roughly the square of the refractive index ( $\varepsilon = n^2$ ).

For metals, the permittivity is <u>complex</u> (energy absorption) and *dispersive* ( $\lambda$  dependent).



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### **The Optical Near-Field**

The absorption and scattering cross sections correspond to the "far field" properties of the nanoparticles, i.e. they describe what happens to a light wave that passed the particle.

One can also talk about the "near-field", i.e. the local electromagnetic field distribution on the nanoscale.

The field is strongest at the metal and typically extends a distance approximately equal to the radius of the particle.

Electrostatic theory can be used to calculate the near field as well:

$$\vec{E}(x,y,z) = E_0 \left[ \vec{x} - \operatorname{Re}(\alpha_0) \left[ \frac{\vec{x}}{r^3} - \frac{3x}{r^5} [x\vec{x} + y\vec{y} + z\vec{z}] \right] \right]$$



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#### **Surface Plasmons**

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Surface plasmons are similar to ordinary light (electromagnetic plane wave) but confined to the <u>interface</u> between a metal (conductor) and a dielectric (insulator).

The surface plasmon <u>propagates</u> along the interface (like a wave on a water surface). Eventually the wave energy has dissipated (normally by heating the metal).



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#### **The Dispersion Relation**

There exists a relation between the <u>momentum</u> and <u>energy</u> of a surface plasmon. In contrast to nanoparticles, surface plasmons exist in a *continuum* of frequencies!

Problem: Momentum is always lacking for the incident light! The dispersion relation does not cross that of photons in the dielectric medium!



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#### **Excitation of Surface Plasmons**

The additional momentum needed can be added in several ways.

One is to introduce a periodic <u>grating</u> on the surface. The grating wavevector adds to that of the incident photons. The condition for excitation is:

$$\operatorname{Re}\left(\sqrt{\frac{\varepsilon(\lambda_0)\varepsilon_{\mathrm{m}}}{\varepsilon(\lambda_0)+\varepsilon_{\mathrm{m}}}}\right) = n_{\mathrm{m}}\sin(\theta) + \frac{j\lambda_0}{\Lambda}$$

One can also use a high refractive index material, a <u>thin</u> metal film and *total internal reflection* configuration. The prism adds to the photon momentum:

$$\operatorname{Re}\left(\sqrt{\frac{\varepsilon(\omega)\varepsilon_{\mathrm{m}}}{\varepsilon(\omega)+\varepsilon_{\mathrm{m}}}}\right) = n_{\mathrm{p}}\sin(\theta)$$



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#### **Total Internal Reflection**

When measuring the reflected light one sees a minimum, representing coupling to surface plasmons!

One can vary either the <u>angle</u> or the <u>wavelength</u> of incident light.



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# **Surface Plasmon Near-Field**

distribution At any time, the surface plasmon has negative and of E field positive poles on the metal surface. The electric field has two components in the xz plane. Magnetic field only in y. The time-averaged field strength only depends on the  $\lambda_{SP}$ distance from the surface.  $1.4 \times 10^7 + 9.7 \times 10^4$ i m<sup>-1</sup>  $k_z = -2.4 \times 10^5 + 5.7 \times 10^6$ i m<sup>-1</sup> z k. electric field component (a.u.) The field extends approximately half of the wavelength of light used to excite the surface plasmon. Aι λsı

position in propagation direction (x,  $\mu$ m)



# **Detection with Plasmons**

The most common plasmonic sensor principle is *refractometric detection*:

• When a molecule binds to the surface, the refractive index changes.

• The properties of the plasmon are changed because they depend on the refractive index close to the metal.

• By optical spectroscopy, changes in intensity of light can then be detected. The resonance will <u>shift</u> in the spectrum (angle or wavelength).

This holds both for surface plasmons and nanoparticle plasmons. The latter normally use wavelength shifts while SPR instruments measure angular shifts.

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#### **Commercial SPR**

• First paper published in 1983.

- Pharmacia Biosensor started shortly after. Became Biacore later, then part of GE Healthcare, then eaten by Cytiva.
- SPR is now the most established technology for studying biomolecular interactions (later lecture).
- SPR has also become popular in material science.

• The instruments are expensive, but primarily because they contain efficient liquid handling and temperature stabilization etc. SPR can be cheap!









Label-free interaction analysis in real time

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# **SPR Imaging**

SPR can be operated in *imaging* mode which enables multiplexing: Several surface reactions can be probed simultaneously using the same sample solution.

Only intensity variations are measured (camera).

Ideal for use with patterned surfaces!





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# **Importance of Field Extension**

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If the electromagnetic field extends very little, molecules far away will not be detected.

If the field extends far, only a part of the detection capability is utilized and the system may be more sensitive to "bulk effects" far away from the surface.



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# **Additional Coatings**

The metal does not have to be gold, but it is good due to chemical stability and low optical absorption.

Thin coatings on top are also possible if they are not too absorbing!



Silicon dioxide surfaces for MP-SPR	
	Sillcon dioxide is one of the most demanded surfaces. It is a good model of glass surfaces. Amongst others, it guarantees formation of supported lipid bilayer.
SPR102-SIO2	SiO2 is deposited on top of our standard Au-sensor slides.
	Available as a pack of 10 pieces.
Other inorganic coating	gs for MP-SPR
The materials are typically deposited on top of gold sensor as they do not have plasmonic properties, which are required for the phenomena to work.	
Typical applications for inorganic materials include photovoltaics, display technologies, food additives and other.	
SPR102-AI2O3	Aluminum oxide coating, available as a pack of 10 pieces
SPR102-ITO	Indium-tin oxide coating, available as a pack of 10 pieces
SPR102-ZNS	Zinc sulfide coating, available as a pack of 10 pieces
SPR102-Hf02	Hafnium oxide coating, available as a pack of 10 pieces
SPR102-TIO2	Titanium dioxide coating, coating, available as a pack of 10 pieces
SPR102-CUST-IO	Interested in another inorganic coating on sensors? Ask us about the availability.
SPR102-CUST-POL	Interested in a polymer coated sensors? Ask us about the availability.
and the second second	Glass substrate Adhesion layer Other material TiOp, Slop, Al <sub>2</sub> O <sub>2</sub> , ITO, ZnS,  Bionavis http://www.bionavis.com/

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# **Miniaturized Nanoparticle Sensors**

If SPR is so great, why bother with plasmonic biosensors based on nanoparticles?

One reason is that they are very small! In SPR, the sensing spot is at least microscale.





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# **Other Optical Techniques**

Plasmons is definitely not the only way to go!

- Ellipsometry.
- Optical waveguide lightmode spectroscopy.
- Dual polarization interferometry.

Very similar since all are based on refractometric detection!



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# **Piezoelectricity**

Some crystalline materials generate electric fields upon deformation because the atoms have different electronegativity.

*Piezoelectricity* is the connection between mechanical and electrical potential energy in a material.

Apply pressure to generate voltage or the other way around!





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### **Quartz Crystal Microbalance**

Gold plates on a quartz crystal deform it in shear mode (for the proper crystal angle cut).

With an AC voltage we can force the crystal into oscillation.

At the *acoustic* resonance frequencies *f* the amplitude is enhanced:

$$f = n\frac{v}{\lambda} = n\frac{v}{2d_0}$$

Here v is the speed of <u>sound</u> (in the material) and n is an integer.

In quartz v = 3340 m/s.

Crystal 334  $\mu$ m thick gives f = 5 MHz for the fundamental resonance (n = 1).



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#### **QCM Sensors**

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Sensing principle is that an adsorbed film becomes part of the oscillation. If a thin film of thickness d is bound to the resonator with initial thickness  $d_0$  the frequency shift is:

$$\Delta f = \frac{nv}{2[d_0 + d]} - \frac{nv}{2d_0} = \frac{nv}{2} \left[ \frac{1}{d_0 + d} - \frac{1}{d_0} \right] = \frac{nv}{2} \times \frac{d_0 - [d_0 + d]}{d_0[d_0 + d]}$$
$$= -\frac{nv}{2} \times \frac{d_0}{d_0[d_0 + d]} = -\frac{nv}{2} \times \frac{1}{d_0[\frac{d_0}{d_0} + 1]} \approx -\frac{nv}{2d_0} \times \frac{d_0}{d_0} = -\frac{f_0}{d_0} \times d$$

The QCM sensor is thus essentially a thickness meter!

Higher  $\Delta f$  for higher  $f_0$ , but also more noise (thinner crystals).





#### **Dissipation Monitoring**

If we excite the oscillation with an AC voltage close to f and then disconnect, the crystal will continue to oscillate freely at its resonance frequency for a short time.

The amplitude A will decay exponentially with a certain dissipation D:

 $A(t) = A_0 \sin(2\pi f t) \exp(-Df t)$ 

Both f and D are obtained. The definition of D is energy loss <u>per cycle</u>, so it is dimensionless.

In liquids D becomes high and:

$$\Delta f = -f_0^{3/2} \left[ \frac{\rho_l \eta_l}{D \rho_q G_q} \right]^{1/2}$$

 $G_{\rm q}$  is the elastic storage modulus of quartz, which is 2.95×10<sup>10</sup> Pa.



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#### **Quantification of Frequency Shift**

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The frequency shift can be rewritten in terms of mass coverage and film density:

$$\Delta f = -\frac{f_0}{d_0} \times d = -\frac{f_0}{d_0} \times \frac{\Gamma M}{\rho}$$

In 1952 a German guy called Sauerbrey said that the adsorbed film can be assumed to have the density of quartz as long as it is <u>rigid</u> and much thinner than the acoustic wavelength. (It kind of makes sense.) This means that:

$$\Delta f = -\frac{f_0}{d_0} \times d = -\frac{f_0}{d_0 \rho_{\rm q}} \times \Gamma M$$

This gives a linear sensitivity and a Sauerbrey constant:

$$S = \frac{d_0 \rho_q}{f_0}$$

For a typical 5 MHz quartz crystal ( $\rho_q = 2.65 \text{ g/cm}^3$ ) becomes  $\underline{17.7 \text{ ng/cm}^2 \text{ per Hz}}$ .

If  $\Delta D/\Delta f > 4 \times 10^{-7}$  Hz<sup>-1</sup> Sauerbrey does not work and the film must be treated as *viscoelastic* (more advanced).

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# "Dry" and "Wet" Mass

Especially for highly hydrated "floppy" molecules on the surface a lot of water will be coupled to the oscillation and thus also detected as mass.

The mass determined by an optical sensor and the QCM differs!

Example: Change in frequency and dissipation when a polymer becomes dehydrated.



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# Video: QCM-D

Generic tool for studies in liquids.



#### **Surface Material Variation**

Just like for SPR, additional coatings can be used on the sensor crystals. It does not have to be gold!

Even more flexibility: the films can be thicker than in SPR and it is not a problem if they are optically absorbing (which kills plasmons). Carbon is one example!



https://www.biolinscientific.com/qsense/sensors

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### **Other Mechanical Sensors**

Microcantilevers can oscillate or bend due to surface binding.



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# **Electrochemical Impedance Spectroscopy**

Electrochemistry can be used to characterize the surface of electrodes and to detect molecular binding.

The method that gives the most information is electrochemical impedance spectroscopy (EIS).

We apply an AC voltage with angular frequency  $\omega = 2\pi f$ :

#### $U(t) = U_0 \sin(\omega t)$

The amplitude is kept low (~10 mV) so that the system responds <u>linearly</u>. The current is then also sinusoidal with a certain amplitude and a *phase shift*  $\varphi$ :

$$I(t) = I_0 \sin(\omega t - \phi)$$

The impedance Z is a more general term than electrical resistance. It is complex and frequency dependent. In principle it is still defined as voltage divided by current:

$$Z = \frac{U_0 \sin(\omega t)}{I_0 \sin(\omega t - \phi)}$$

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#### **Complex Denotation**

Everything becomes easier if we use Euler's formula:

 $U = U_0 \exp(\mathrm{i}\omega t)$ 

 $I = I_0 \exp(\mathrm{i}[\omega t - \phi])$ 

The impedance is then represented by a *magnitude*  $Z_0$  (of the complex number) and a *phase*  $\varphi$ :



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#### **Circuit Elements**

An ideal resistor has no capacitive effects and Z is real with no dependence on  $\omega$ :

$$Z = \frac{U_0}{I_0} = Z_0 = R$$

An ideal capacitor has zero steady state current and Z is purely imaginary:

$$Z = Z_0 \exp\left(i\frac{\pi}{2}\right) = -\frac{i}{\omega C}$$

We can combine impedances (just like resistors). Resistor and capacitor in series:



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#### **Impedance Spectra**

EIS data can be visualized in the complex plane (Nyquist plot), but to see the frequency dependence more clearly a *Bode plot* of  $Z_0(\omega)$  and  $\varphi(\omega)$  (double y-axis) is usually better.





#### **Equivalent Circuits**

So what is the relation to surface analysis? EIS data can be modelled by *equivalent circuits*, i.e. elements like resistors and capacitors (even though the real system is not like that at all).

We can distinguish from *charge transfer* (Faradaic reactions) and *capacitive currents* (typically the double layer). We will always have both at the surface!

Especially with a redox active molecule in solution, EIS will detect if something binds to the surface. Changes in double layer capacitance can also be detected.



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#### **Other Electrical Techniques**

Field effect sensors monitor changes in conductivity.

Many versions exist, such as nanowires. They essentially respond to charge of analytes.

Do not work well at physiological ionic strength because of screening.



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#### Conclusions

Surface sensitive techniques are generic tools that detects binding of <u>all</u> molecules to surfaces <u>without</u> any chemical identification.

They normally provide data in real-time so you can get information of rate constants.

Signal transduction is normally based on something of the following:

- Refractive index (optical sensors).
- Mass (mechanical sensors).
- Charge (electrical sensors).

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#### **Implications from Binding Kinetics**

Remember the models for binding kinetics to surfaces!

If the surface is a sensor that gives a measurable response proportional to  $\Gamma$  (e.g. SPR and QCM)

• Real-time operation gives  $k_{on}$  and  $k_{off}$  and confirms equilibrium. Measuring the equilibrium coverage gives only  $K_D$  from  $C_0$  or vice versa.

• Diffusion models can estimate mass coverage limits: A molecule can diffuse to the sensor surface without binding to it, but not bind to the surface without first diffusing to it.

• Flow is often needed to prevent diffusion effects and reach Langmuir behavior. The depletion zone needs to be eliminated!



#### **Checklist 3**

- · Plasmons in nanoparticles: absorption and scattering
- · Electrostatic approximation as well as near-field vs far-field
- Plasmons on surfaces, dispersion relations and excitation mechanisms
- Piezoelectricity
- Quartz crystal microbalance principle of detection
- The dissipation parameter
- The "wet" mass (vs dry mass)
- Impedance spectrum measurements
- · Capacitive and resistive contributions in electrochemistry

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#### Exercise 3.1

A SPR sensor monitors the resonance wavelength  $\lambda_{res}$ , which changes with the refractive index of the environment (*n*) according to  $\lambda_{res} = S_0 n$ , where  $S_0 = 10^4$  nm (per refractive index unit). The refractive index change from proteins in water is 0.185 mL/g (unit is inverse concentration). A protein binds to the surface and forms a 10 nm thick film. What is  $\Gamma$  (here in mass per area) if the experiment shows  $\Delta \lambda_{res} = 5$  nm? Assume that the sensitivity distribution follows a one dimensional exponential decay with  $\delta = 100$  nm:

$$\Delta\lambda_{\rm res} = \frac{S_0}{\delta} \int_0^\infty \Delta n(z) \exp\left(-\frac{z}{\delta}\right) dz$$

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#### Exercise 3.1

We need to calculate the refractive index change in the thin film based on the SPR response. The idea is that  $\Delta n$  is constant in the film and zero otherwise:

$$\Delta\lambda_{\rm res} = \frac{\Delta n S_0}{\delta} \int_0^{10} \exp\left(-\frac{z}{\delta}\right) dz = \frac{\Delta n \times 10^4}{\delta} \left\{-\delta \times \exp\left(-\frac{z}{100}\right)\right\}_0^{10} = \Delta n \times 10^4 \left[1 - \exp\left(-\frac{10}{100}\right)\right]$$

This gives  $\Delta n = 0.0053$  inside the 10 nm film. The concentration of proteins is then 0.0053/0.185 = 0.0284 g/cm<sup>3</sup>. To get the surface coverage we multiply with the thickness (10 nm):

$$\Gamma = 0.0284 \frac{g}{cm^3} \times 10 \times 10^{-7} cm = 2.84 ... \times 10^{-8} \frac{g}{cm^2} = 28 \frac{ng}{cm^2}$$

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#### Exercise 3.2

A QCM sensor detects colloidal particles adsorbing to the sensor surface. The noise level in the measurement is 1 Hz. The colloids are spherical polystyrene particles 100 nm in diameter ( $\rho = 1.04 \text{ g/cm}^3$ ). What is the lowest number of particles on 1  $\mu$ m<sup>2</sup> that the system can detect? You can use the Sauerbrey relation, but comment on the main error!



#### Exercise 3.2

We translate the noise level into a surface coverage by Sauerbrey:

 $\Gamma M = \Delta f \times S = 17.7 \text{ ng/cm}^2 = 1.77 \times 10^{-16} \text{g/}\mu\text{m}^2$ 

How many particles correspond to this mass? Each particle has a weight of  $4\pi R^{3}/3 \times 1.04 \text{ g/cm}^{3} = 5.4 \times 10^{-16} \text{ g}$ , so it is enough with 0.32 particles per  $\mu m^{2}$ .

The particles are solid so probably  $\Delta D$  is low, but each particle still gives a higher signal than that corresponding to its mass because of <u>coupled solvent</u>!



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#### **Exercise 3.3**

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EIS is useful but it is complicated to interpret and analyze results. At an electrode interface, it is easy to see that both capacitive and Faradaic processes occur by just applying a DC voltage  $U_0$ . For a simple capacitor and resistor in parallel, the current is then expected to change as:

 $I(t) = I_0 \exp(-kt) + I_{\rm ss}$ 

The voltage is applied at t = 0.

Draw the I(t) function and explain how to obtain R and C from such data!



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### Exercise 3.3

After sufficient time, the capacitor is fully charged and the current goes only through the resistor. This current corresponds to  $I_{\rm ss}$ , so R =  $U_0/I_{\rm ss}$ .

The capacitance can be obtained by integrating the function I(t) in time, but you must subtract the contribution from the resistor ( $I_{ss}$ ). This gives the total charge Q stored in the capacitor. The capacitance is then  $C = Q/U_0$ .



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